

# Intrinsic Gating Properties of a Cloned G Protein-activated Inward Rectifier K<sup>+</sup> Channel

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**ABSTRACT** The voltage-, time-, and K<sup>+</sup>-dependent properties of a G protein-activated inwardly rectifying K<sup>+</sup> channel (GIRK1/KGA/Kir3.1) cloned from rat atrium were studied in *Xenopus* oocytes under two-electrode voltage clamp. During maintained G protein activation and in the presence of high external K<sup>+</sup> ( $V_K = 0$  mV), voltage jumps from  $V_K$  to negative membrane potentials activated inward GIRK1 K<sup>+</sup> currents with three distinct time-resolved current components. GIRK1 current activation consisted of an instantaneous component that was followed by two components with time constants  $\tau_f \sim 50$  ms and  $\tau_s \sim 400$  ms. These activation time constants were weakly voltage dependent, increasing approximately twofold with maximal hyperpolarization from  $V_K$ . Voltage-dependent GIRK1 availability, revealed by tail currents at  $-80$  mV after long prepulses, was greatest at potentials negative to  $V_K$  and declined to a plateau of approximately half the maximal level at positive voltages. Voltage-dependent GIRK1 availability shifted with  $V_K$  and was half maximal at  $V_K - 20$  mV; the equivalent gating charge was  $\sim 1.6 e^-$ . The voltage-dependent gating parameters of GIRK1 did not significantly differ for G protein activation by three heterologously expressed signaling pathways: m2 muscarinic receptors, serotonin 1A receptors, or G protein  $\beta 1\gamma 2$  subunits. Voltage dependence was also unaffected by agonist concentration. These results indicate that the voltage-dependent gating properties of GIRK1 are not due to extrinsic factors such as agonist-receptor interactions and G protein-channel coupling, but instead are analogous to the intrinsic gating behaviors of other inwardly rectifying K<sup>+</sup> channels.

## INTRODUCTION

Inwardly rectifying K<sup>+</sup> channels ( $K_{ir}$  channels) activated by G protein-coupled receptors decrease membrane excitability by hyperpolarizing the membrane potential, slowing membrane depolarization, and shortening the action potential waveform. These tightly regulated  $K_{ir}$  channels are functionally expressed in the heart (Kurachi, Tung, Ito, and Nakajima, 1992) and various neurons of the central nervous system (North, 1989), with the best characterized example being the acetyl-

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choline (ACh)-activated  $K_{ir}$  channel ( $K_{ACh}$  channel) expressed in atrial pacemaker cells and myocytes.

Activation of m2 muscarinic receptors on atrial myocytes results in an increase in the probability of  $K_{ACh}$  channel opening via a direct membrane-delimited signaling pathway that involves heterotrimeric G proteins (Soejima and Noma, 1984; Breitwieser and Szabo, 1985; Pfaffinger, Martin, Hunter, Nathanson, and Hille, 1985). After the initial controversy over whether pertussis toxin-sensitive  $G\alpha$  subunits (Codina, Yatani, Grenet, Brown, and Birnbaumer, 1987; Yatani, Mattera, Codina, Graf, Okabe, Podrell, Iyengar, Brown, and Birnbaumer, 1988) or  $G_{\beta\gamma}$  heterodimers (Logothetis, Kurachi, Galper, Neer, and Clapham, 1987; Logothetis, Kim, Northrup, Neer, and Clapham, 1988) mediate the membrane-delimited signaling, it now appears clear that G protein- $K_{ACh}$  channel coupling involves primarily  $G_{\beta\gamma}$  dimers (Ito, Tung, Sugimoto, Koboyashi, Takahashi, Katada, Ui, and Kurachi, 1992; Wickman, Inlguez-Lluhl, Davenport, Taussig, Krapivinsky, Linder, Gilman, and Clapham, 1994; Yamada, Ho, Lee, Kontani, Takahashi, Katada, and Kurachi, 1994).

$K_{ACh}$  channel activation by  $G_{\beta\gamma}$  subunits represents the primary step in  $K_{ACh}$  channel gating. During steady state G protein activation,  $K_{ACh}$  channel currents ( $I_{K_{ACh}}$ ) also display several distinct voltage- and time-dependent gating properties. The foremost of these is inward rectification, mediated by voltage-dependent intracellular  $Mg^{2+}$  block (Horie and Irisawa, 1987, 1989) and by voltage-dependent channel gating (Noma and Trautwein, 1978; Sakmann, Noma, and Trautwein, 1983; Iijima, Irisawa, and Kameyama, 1985; Horie and Irisawa, 1987; Simmons and Hartzell, 1987). In response to voltage steps,  $I_{K_{ACh}}$  exhibits relaxations on a time scale of several hundred milliseconds that qualitatively resemble the "intrinsic" voltage-dependent gating processes described for several constitutively active invertebrate (Hagiwara, Miyazaki, and Rosenthal, 1976; Gunning, 1983) and vertebrate (Leech and Stanfield, 1981; Kurachi, 1985; Silver and DeCoursey, 1990)  $K_{ir}$  channels. The time-dependent increase in inward  $K_{ir}$  current during hyperpolarizing voltage steps from the  $K^+$  equilibrium potential ( $V_K$ ) is termed "activation," and the time-dependent decrease in outward current during voltage steps positive to  $V_K$  is referred to as "deactivation." Constitutively active mammalian  $K_{ir}$  currents typically display activation and deactivation on a much faster time scale ( $<10$  ms) than that for  $I_{K_{ACh}}$ . Additionally, the gating of constitutively active  $K_{ir}$  currents shifts relative to  $V_K$ . This property, common among  $K_{ir}$  channels, suggests that  $K^+$  binding is an integral step in the gating process (Hille and Schwarz, 1978; Ciani, Krasne, Miyazaki, and Hagiwara, 1978). In this respect, the voltage and  $K^+$  dependence of  $I_{K_{ACh}}$  activation/deactivation has not been fully characterized.

Here we describe the voltage, time, and  $K^+$  dependence of a G protein-activated  $K_{ir}$  channel (GIRK1/KGA/Kir3.1) recently cloned from rat atrium (Dascal, Schreiblemeyer, Lim, Wang, Chaukin, DiMagno, Labarca, Kieffer, Gaveriaux, Trollinger, Lester, and Davidson, 1993; Kubo, Reuveny, Stesinger, Jan, and Jan, 1993). As in native atrial myocytes, GIRK1 displays slow voltage-dependent activation and steep inward rectification when expressed in *Xenopus* oocytes (Kubo et al., 1993). In the present report, G protein-mediated activation of GIRK1 was initiated in *Xenopus* oocytes by several manipulations involving other coexpressed proteins. The hu-

man m2 receptor and the human serotonin 1A (5-HT<sub>1A</sub>) receptor activated GIRK1 via endogenous oocyte G proteins; and heterologously expressed G protein  $\beta_1\gamma_2$  subunits ( $G_{\beta_1\gamma_2}$ ) activated GIRK1 directly. Our results indicate that the slow voltage-dependent gating of GIRK1 currents represents an intrinsic channel gating process that is independent of the signaling steps leading to channel activation (i.e., agonist-receptor coupling and G protein-channel coupling). As for other  $K_{ir}$  channels, the voltage dependence of GIRK1 intrinsic gating depends on external  $K^+$ . The rate constants of GIRK1 activation/deactivation, however, are only weakly voltage dependent in contrast to the steep voltage dependence described for other  $K_{ir}$  channels.

The details of  $I_{K_{ACh}}$  activation and deactivation are interesting as channel gating phenomena but may also be physiologically important. In the heart, these kinetics could determine the shortening of action potential durations and the preservation of intracellular  $K^+$  levels during the long plateau phase of the cardiac action potential (Horie and Irisawa, 1987). The voltage-dependent gating properties of these  $K_{ir}$  channels may also be important in modulating excitability of central and peripheral neurons (North, 1989). Some of these results were presented in abstract form elsewhere (Doupnik, Lim, Schreibley, Dascal, Davidson, and Lester, 1994a).

## MATERIALS AND METHODS

### *Clones and cRNA*

GIRK1 and the human 5-HT<sub>1A</sub> receptor (provided by P. Hartig, Synaptic Pharmaceuticals Corp.) were cloned in pBluescript II KS (–) (Stratagene, La Jolla, CA). The human m2 receptor (provided by E. Peralta, Harvard University, Cambridge, MA) was cloned in pGEM3Z (Promega Corp., Madison, WI).  $G_{\beta_1}$  and  $G_{\gamma_2}$  were cloned in pFroggy (provided by A. Connolly and S. Coughlin, University of California, San Francisco), a derivative of pCDM8 (Invitrogen Corp., San Diego, CA), in which the G protein gene is flanked by both the 5' and 3' untranslated regions of the *Xenopus*  $\beta$ -globin gene. cRNA was transcribed in vitro by T7 or SP6 RNA polymerase (MEGAscript; Ambion, Austin, TX) from linearized cDNA.

### *Preparation of Oocytes and cRNA Injection*

Immature stage V and VI oocytes from *Xenopus laevis* were enzymatically dissociated from resected ovarian tissue as described elsewhere (Quick and Lester, 1994). Isolated oocytes were maintained at 19°C in a modified Barth's medium of the following composition (in millimolar): 96 NaCl, 2 KCl, 1 CaCl<sub>2</sub>, 1 MgCl<sub>2</sub>, 5 HEPES (*N*-[2-hydroxyethyl]piperazine-*N'*-[2-ethanesulfonic acid]), 2.5 sodium pyruvate, 0.5 theophylline, 50  $\mu$ g/ml gentamicin, pH 7.5 (NaOH). The incubation medium was changed on a daily basis.

Oocytes were coinjected with 1 ng of GIRK1 cRNA and either 0.5 ng of m2 receptor cRNA, 4 ng of 5-HT<sub>1A</sub> receptor cRNA, or 1 ng of both  $G_{\beta_1}$  and  $G_{\gamma_2}$  cRNAs in RNase-free H<sub>2</sub>O. The final injection volume was 50 nl in all cases. Electrophysiological experiments were performed 4–7 d after injection.

### *Electrophysiological Recordings*

Two-electrode voltage clamping of *Xenopus* oocytes was performed at 19–21°C with an Axoclamp 2A amplifier (Axon Instruments, Inc., Foster City, CA). The voltage recording and current-injecting microelectrodes were filled with 3 M KCl and had tip resistances of 0.8–1.2 M $\Omega$ . Transmem-

brane potential was measured differentially between the intracellular electrode and a bath electrode in order to minimize series resistance artifacts. The bath electrodes consisted of Ag/AgCl pellets positioned between the oocyte and the suction/output line of the perfusion chamber. Data acquisition and voltage command signals were executed using pCLAMP software (version 5.5.1; Axon Instruments, Inc.) and a microcomputer. Unless otherwise indicated, current signals were low pass filtered at 200 Hz (−3 dB) with an eight-pole Bessel-type filter (Frequency Devices Inc., Haverhill, MA) and digitized at 400 Hz during pCLAMP episodes. The current signal was also continuously recorded on an analogue strip chart recorder. For cumulative dose-response experiments, currents were digitized at 1 Hz and acquired using AxoTape software (Axon Instruments, Inc.). Current analysis and nonlinear curve fitting were performed with pCLAMP and NFITS software (Island Products, Inc., Galveston, TX).

### *Solutions and Drugs*

During electrophysiological recordings, oocytes were continuously superfused with  $\text{Ca}^{2+}$ -free solutions to reduce the  $\text{Ca}^{2+}$ -activated  $\text{Cl}^-$  current ( $I_{\text{Cl}(\text{Ca})}$ ) endogenous to *Xenopus* oocytes (Dascal, 1987). Initially, oocytes were superfused with ND98 solution, which consisted of (in millimolar): 98 NaCl, 1  $\text{MgCl}_2$ , and 5 HEPES, pH 7.5 (NaOH). To record inward  $\text{K}^+$  currents, the recording chamber perfusion was switched to a high  $\text{K}^+$  (hK) solution that was identical to ND98 with the exception that NaCl was replaced with 98 mM KCl. Rapid activation of heterologously expressed G protein-coupled receptors was accomplished by applying the appropriate receptor agonist in hK solution via a U-tube superfusion apparatus (Bormann, 1992). The exchange rate for the external solution surrounding the oocyte was  $<1$  s, as determined by the time course for ACh activation of heterologously expressed nicotinic ACh receptors (Cohen, Figl, Quick, Labarca, Davidson, and Lester, 1995). A manifold at the input of the U-tube allowed for multiple agonist concentration changes with a minimal delay ( $\sim 1$  s) due to tube dead space.

In several batches of oocytes, ACh superfusion activated  $I_{\text{Cl}(\text{Ca})}$  presumably by causing intracellular  $\text{Ca}^{2+}$  release via m2 receptor activation (Lechleiter, Girard, Clapham, and Peralta, 1991) and/or activation of an endogenous muscarinic receptor (see Dascal, 1987). Oocytes were therefore routinely incubated for  $\sim 30$  min in 100  $\mu\text{M}$  BAPTA/AM (1,2-bis-[*o*-aminophenoxy]-ethane-*N,N,N',N'*-tetraacetic acid tetra-[acetoxymethyl]-ester), a membrane-permeant  $\text{Ca}^{2+}$  chelator. The BAPTA/AM incubation effectively eliminated ACh activation of  $I_{\text{Cl}(\text{Ca})}$  and reduced the resting membrane conductance of the oocyte.

BAPTA/AM (Calbiochem, San Diego, CA) was made up as a stock concentration of 10 mM dissolved in dimethylsulfoxide and stored in aliquots in darkness at  $-23^\circ\text{C}$ . ACh and 5-HT (Sigma Chemical Co., St. Louis, MO) were also made up in concentrated stock solutions (in  $\text{H}_2\text{O}$ ) that were stored as frozen aliquots at  $-23^\circ\text{C}$ . All reagents were thawed and used fresh the day of the experiment.

## RESULTS

### *Voltage-Jump Relaxations of GIRK1 Currents*

In voltage clamped *Xenopus* oocytes ( $V_m = -80$  mV) coexpressing GIRK1 and the m2 receptor, 1  $\mu\text{M}$  ACh activated an inward current ( $I_{\text{K,ACh}}$ ) in the presence of high external  $\text{K}^+$  (98 mM). The ACh-activated current desensitized partially over a time course of minutes in the continued presence of agonist (Fig. 1 A). Previous studies showed that  $I_{\text{K,ACh}}$  is highly selective for  $\text{K}^+$  ions, exhibits  $[\text{Mg}^{2+}]_i$ -dependent inward rectification, is dependent on receptor activated G proteins, and is sensitive to external  $\text{Ba}^{2+}$  block (Dascal et al., 1993; Kubo et al., 1993). To study the voltage-

dependent properties of  $I_{K,ACh}$ , voltage jumps to varying membrane potentials were evoked in high external  $K^+$  in the absence and presence of ACh.  $I_{K,ACh}$  was then isolated by digital subtraction of the currents in these two conditions (Fig. 1 B). The resulting steady state  $I_{K,ACh}(V)$  relation displays (a) steep inward rectification and (b) a reversal potential ( $V_{rev}$ ) near the predicted  $V_K$  of  $\sim 0$  mV (Fig. 1 C). The lack of

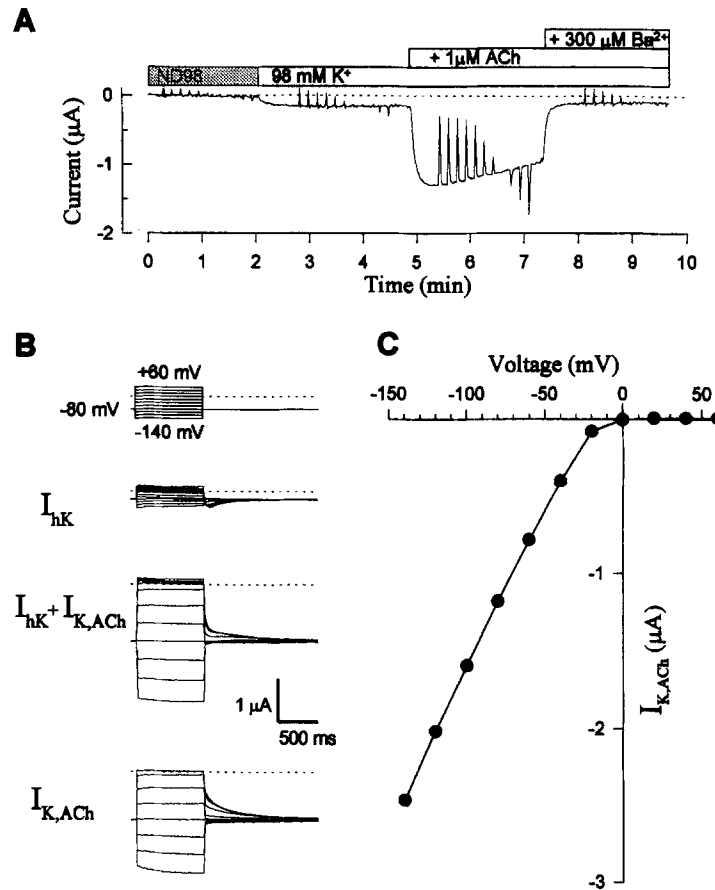


FIGURE 1. Isolation of  $I_{K,ACh}$  in a *Xenopus* oocyte coexpressing the m2 receptor and GIRK1. (A) Voltage clamp currents at a holding potential of  $-80$  mV. The oocyte was first superfused with a  $98$  mM  $K^+$  solution, which evoked a small inward current ( $\sim 100$  nA;  $I_{hK}$ ) caused by both an endogenous  $K_{ir}$  current and the agonist-independent activity of GIRK1 (Lim et al., 1994). ACh ( $1$  μM) application evoked a much larger inward  $I_{K,ACh}$  ( $\sim 1.4$  μA) that was completely blocked by  $300$  μM  $Ba^{2+}$ . The spikes in the current record are currents evoked by the voltage jumps described in B. (B) Superimposed currents evoked by  $900$ -ms voltage steps at  $0.1$  Hz to varying membrane potentials, before (upper traces;  $I_{hK}$ ) and during (middle traces;  $I_{hK} + I_{K,ACh}$ ) ACh application.  $I_{K,ACh}$  (lower traces) was isolated by digital subtraction of the upper traces from the middle traces. (Dotted line) Indicates the 0-current level for each family of traces. Capacitive transients have been blanked out. (C) Steady state  $I_{K,ACh}(V)$  relation.  $I_{K,ACh}$  amplitudes were measured isochronally near the end of the voltage step. Note the steep inward rectification of GIRK1 currents expressed in *Xenopus* oocytes.

significant outward  $I_{K_{ACh}}$  may be attributable to high internal levels of  $Mg^{2+}$  (Kubo et al., 1993) or polyamines (Ficker, Taglialatela, Wible, Henley, and Brown, 1994; Lopatin, Makhina, and Nichols, 1994; Fakler, Brandle, Bond, Glowatzki, Koenig, Adelman, Zenner, and Ruppersberg, 1994) that block outward  $K_r$  currents. To compensate for  $I_{K_{ACh}}$  desensitization during the execution of various voltage protocols, each current trace was scaled by a "desensitization factor" calculated by dividing the current amplitude at  $-80$  mV of the first jump in the series by the corresponding current amplitude for each trace. This factor ranged between 1 and 1.35. We found that the degree of desensitization did not affect the  $I_{K_{ACh}}$  relaxation properties, because very similar time constants were obtained by (a) repeated volt-

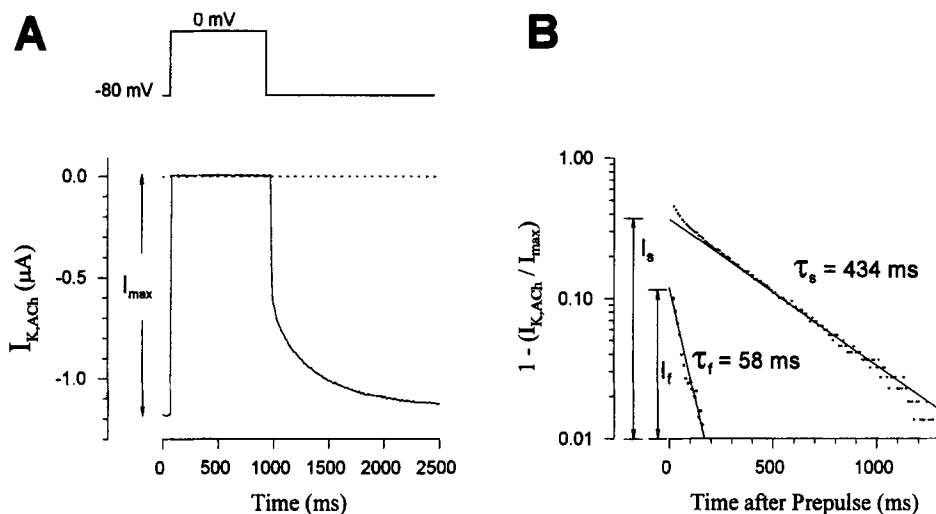


FIGURE 2. Analysis of voltage-jump relaxation currents for GIRK1. (A)  $I_{K_{ACh}}$  activation during a hyperpolarizing step to  $-80$  mV after a  $900$ -ms depolarizing prepulse to  $0$  mV.  $I_{K_{ACh}}$  was isolated as in Fig. 1 B. (B) Semilogarithmic plot of the  $I_{K_{ACh}}$  relaxation for the voltage jump from  $0$  to  $-80$  mV in A. The relaxation was separated into three kinetic components termed instantaneous ( $I_s$ ), fast ( $I_f$ ), and slow ( $I_s$ ), which sum to  $I_{K_{ACh}}$ . For the fast and slow components, the slope of the line gives the rate constants  $\tau_f^{-1}$  and  $\tau_s^{-1}$ , respectively; and extrapolation to the time of the voltage step gives their respective amplitudes.

age jumps at varying times during application of ACh or by (b) reversed voltage pulse sequences.

#### *Time-dependent Kinetics of GIRK1 (Re)activation and Deactivation*

Within the time resolution of our voltage clamp circuit ( $\sim 5$  ms), voltage jumps from a holding potential of  $-80$  mV to positive test potentials resulted in instantaneous changes in  $I_{K_{ACh}}$ , followed by relatively small outward currents ( $< 100$  nA). Similarly, voltage jumps to negative test potentials also resulted in instantaneous changes in  $I_{K_{ACh}}$ , followed by nearly time-invariant currents. The currents changed

by <10% during the 900-ms voltage steps, although some activation and deactivation could be observed with steps to -140 and -20 mV, respectively (see Fig. 1 B). However, upon repolarization to -80 mV from a positive prepulse potential,  $I_{K_{ACh}}$  reactivated much more slowly. The kinetics of the reactivation were dependent on both prepulse voltage and prepulse duration. Waveforms of  $I_{K_{ACh}}$  activation are shown in Fig. 2 and were described by the following relation:

$$I_{K_{ACh}}(t) = I_i + I_f \exp(-t/\tau_f) + I_s \exp(-t/\tau_s) \quad (1)$$

characterizing three distinct components of GIRK1 activation. After a 900-ms prepulse to 0 mV ( $\sim V_K$ ),  $I_{K_{ACh}}$  reactivation began with an initial instantaneous com-

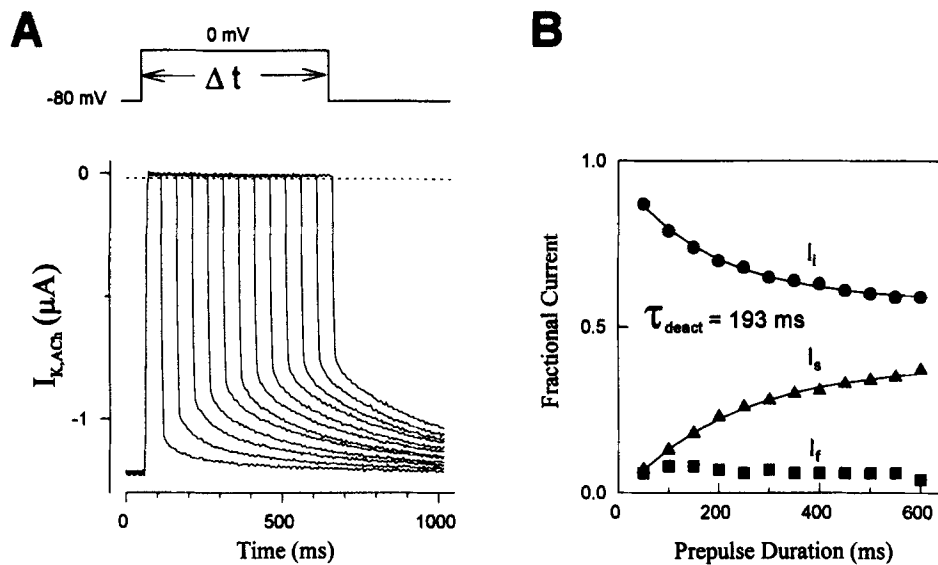


FIGURE 3. Analysis of  $I_{K_{ACh}}$  deactivation. (A) Effects of prepulse duration on  $I_{K_{ACh}}$  activation kinetics. Depolarizing prepulses to 0 mV were given for varying durations at increments of 50 ms, followed by repolarization to -80 mV. Relaxations during the repolarization were analyzed as in Fig. 2. Episodes were evoked at intervals of 10 s. (B) Fractional amplitudes of  $I_i$  (circles),  $I_f$  (squares), and  $I_s$  (triangles) at -80 mV as a function of the prepulse duration ( $\Delta t$ ) at 0 mV. The solid curves through  $I_i$  and  $I_s$  are single exponential fits to the respective data points with a common time constant ( $\tau_{deact}$ ) of 193 ms.

ponent ( $I_i$ ) that represented  $\sim 50\%$  of the  $I_{K_{ACh}}$  amplitude. The two subsequent components to the voltage-jump relaxations were kinetically resolvable. The faster component ( $I_f$ ) had a time constant ( $\tau_f$ ) of  $\sim 50$  ms and comprised  $\sim 15\%$  of the current amplitude, and the slower component ( $I_s$ ) had a time constant ( $\tau_s$ ) of  $\sim 400$  ms and accounted for  $\sim 35\%$  of the  $I_{K_{ACh}}$  amplitude. Prepulse voltage did not affect  $\tau_f$  or  $\tau_s$ , but markedly affected  $I_i$ ,  $I_f$ , and  $I_s$  (described in the following discussion).

The effects of prepulse duration on the kinetics of  $I_{K_{ACh}}$  activation are shown in Fig. 3. Fig. 3 A demonstrates that after a 50-ms prepulse to 0 mV ( $\sim V_K$ ),  $I_{K_{ACh}}$  reactivation was largely instantaneous with a <10% contribution of  $I_s$ . Prepulses of in-

creasing duration increased  $I_i$  at the expense of  $I_f$  (Fig. 3 *B*). The time constant of the "envelope current" corresponding to slow channel deactivation ( $\tau_{\text{deact}}$ ) was  $220 \pm 40$  ms (mean  $\pm$  SD,  $n = 5$ ) with prepulses to 0 mV and  $242 \pm 58$  ms ( $n = 4$ ) with prepulses to +20 mV. In one experiment with prepulses to +60 mV,  $\tau_{\text{deact}}$  was 183 ms. Thus, the rate of slow deactivation showed little or no dependence on prepulse potential in the positive voltage range. With prepulses >600 ms in duration, the decrease in  $I_i$  approached a plateau at an amplitude  $\sim 50\%$  of the total relaxation. Therefore, in the activation studies with 900-ms prepulses (see Fig. 6), channel deactivation was nearly at steady state. In another experiment that achieved steady state deactivation, we set the holding potential to 0 mV rather than

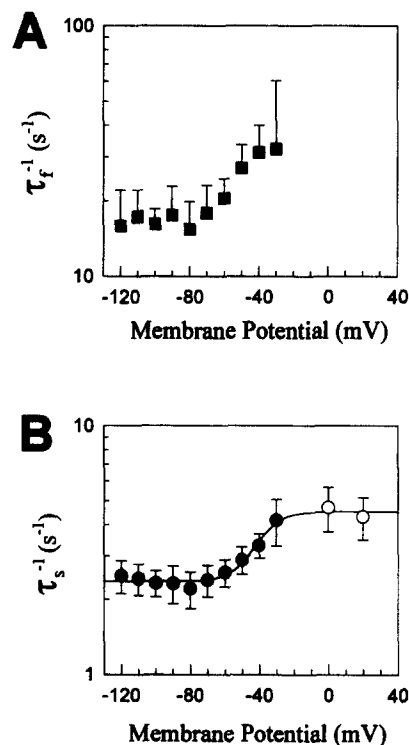


FIGURE 4. Voltage dependence of GIRK1 activation/deactivation. Semilogarithmic plots of (A)  $\tau_f^{-1}$ , the fast rate constant, and (B)  $\tau_s^{-1}$ , the slow rate constant (mean  $\pm$  SD, five oocytes). In B, the closed symbols represent measurements of activation time constants obtained from experiments like that of Fig. 2; the open circles represent the slow deactivation rates from experiments like that of Fig. 3. The solid curve in B is a Boltzmann function fit to the mean data points:  $\tau_s^{-1}$  (V) =  $4.53 - 2.17/[1 + \exp[(E_m + 40)/7.4]]$ .

the usual value of  $-80$  mV and evoked 900-ms test pulses at intervals of 10 s.  $I_{\text{KACH}}$  evoked by hyperpolarizing steps to  $-80$  mV consisted of the three activation components ( $I_f$ ,  $I_s$ , and  $I_i$ ) in the same fractional ratio (0.50:0.15:0.35, respectively) as reactivation after a 900-ms prepulse to 0 mV.

The amplitude of the fast activation component was unaffected by the prepulse durations tested (Fig. 3 *B*) and therefore apparently reaches a steady state level of deactivation within the shortest pulse we used (50 ms). We did not systematically study the influence of shorter depolarizing prepulses on the fast component of activation, because this component constitutes a relatively small fraction of the total relaxation amplitude.



### Voltage Dependence of GIRK1 Activation/Deactivation Rates

To examine the voltage dependence of  $\tau_f$  and  $\tau_s$ , we used a 900-ms depolarizing prepulse to 0 mV;  $I_{K_{ACh}}$  reactivation was then elicited by voltage steps to varying negative test potentials. Fig. 4 shows the rate constants for  $I_{K_{ACh}}$  activation/deactivation ( $\tau_f^{-1}$  and  $\tau_s^{-1}$ ) as a function of membrane potential. Both  $\tau_f^{-1}$  and  $\tau_s^{-1}$  decrease two- to threefold with hyperpolarization between 0 and  $-80$  mV. In contrast to the characteristic steeply voltage-dependent activation/deactivation rate constants of other  $K_{ir}$  channels (Kurachi, 1985; Saigusa and Matsuda, 1988; Silver and DeCoursey, 1990), GIRK1 activation/deactivation rates followed a monotonic, sig-

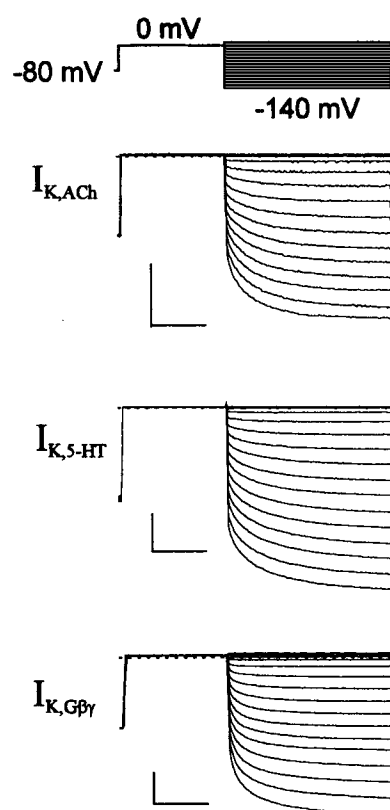


FIGURE 5. Activation of GIRK1 currents during steady state signaling by three different pathways. Traces are from oocytes expressing GIRK1 as well as either m2 receptors ( $I_{K_{ACh}}$ ), 5-HT<sub>1A</sub> receptors ( $I_{K_{5-HT}}$ ), or Gβ1γ2 ( $I_{K_{Gβγ}}$ ). Voltage was stepped to various levels after a 900-ms depolarizing prepulse to 0 mV.  $I_{K_{ACh}}$  and  $I_{K_{5-HT}}$  were evoked by agonists (1  $\mu$ M ACh and 100 nM 5-HT, respectively); whereas  $I_{K_{Gβγ}}$  represents currents in high K<sup>+</sup> ( $I_{hK}$ ) minus those in the additional presence of 300  $\mu$ M Ba<sup>2+</sup>. Calibration bars denote 0.5  $\mu$ A and 500 ms.

moidal relation. Although  $\tau_f^{-1}$  and  $\tau_s^{-1}$  are weakly voltage dependent over most of the voltage range studied, the  $\tau_s^{-1}$  (V) relation displayed a relatively steep transition. In Fig. 4 B, we have fit the data to the sum of a voltage-independent term plus a Boltzmann-type voltage-dependent term having a half-maximal potential at  $-40$  mV and a slope factor of 7.4 mV/ $e$ -fold change.

### GIRK1 Kinetics Do Not Depend on the G Protein Activation Pathway

We examined the GIRK1 voltage-jump relaxation kinetics for various methods of G protein activation (Fig. 5), including m2 muscarinic receptors, 5-HT<sub>1A</sub> receptors,

and  $G_{\beta 1\gamma 2}$  expression. After a 900-ms depolarizing prepulse to 0 mV, GIRK1 activation was elicited by voltage steps to varying negative test potentials. For the case of  $G_{\beta 1\gamma 2}$  expression, GIRK1 currents were isolated by subtraction of currents in the presence of 300  $\mu\text{M}$   $\text{Ba}^{2+}$ , which blocks all of the GIRK1 current but little of the endogenous hK current (see Fig. 1 A). The voltage-jump relaxation waveforms for the various methods were not significantly different from each other, suggesting that voltage-dependent gating occurs at a point distal to the receptor-G protein activation step.

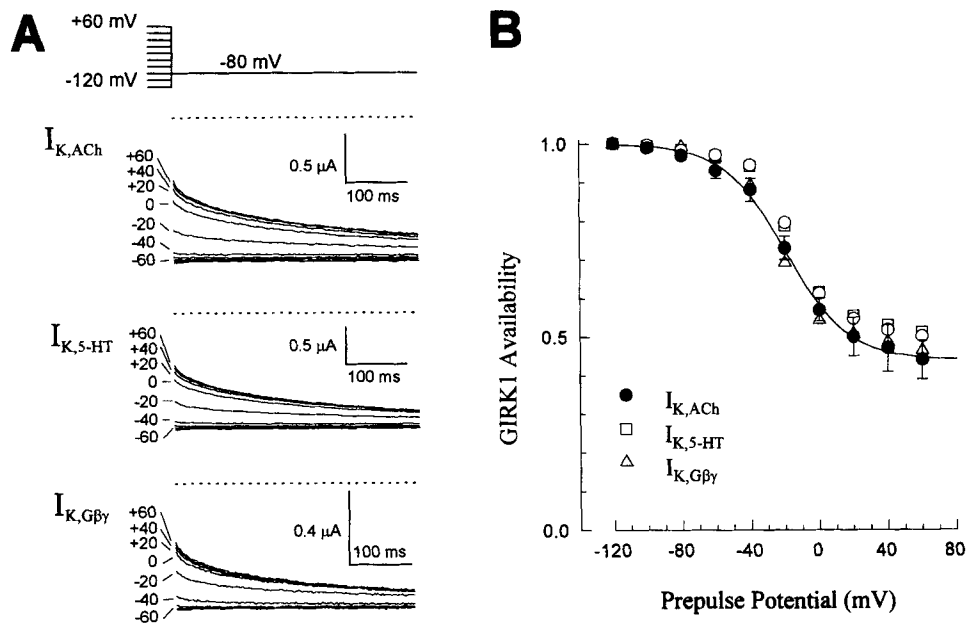


FIGURE 6. Tail current analysis of voltage-dependent GIRK1 availability. (A) GIRK1 tail currents during voltage steps to  $-80$  mV after 900-ms prepulses to varying membrane potentials. GIRK1 was activated either by m2 receptors (*upper traces*), by 5-HT<sub>1A</sub> receptors (*middle traces*), or by  $G\beta 1\gamma 2$  expression (*lower traces*). The dotted line above each family of tail currents is the 0-current level for the oocyte. (B) Voltage-dependent availability curves for  $I_{K,ACh}$  (*open circles*),  $I_{K,5-HT}$  (*open squares*), and  $I_{K,G\beta\gamma}$  (*open triangles*). Isochronal tail current amplitudes at 10–14 ms after the prepulse step were normalized to the maximal amplitude elicited after prepulses to  $-120$  mV. The solid curve is a Boltzmann function fit to the mean  $I_{K,ACh}$  values (*filled circles*,  $\pm$ SD, six oocytes). The availability curves for  $I_{K,5-HT}$  and  $I_{K,G\beta\gamma}$  superimpose on that for  $I_{K,ACh}$ .

#### Tail Current Analysis of Voltage-dependent GIRK1 Availability

Records like those of Fig. 3 indicate that GIRK1 undergoes time-dependent transitions, namely deactivation, at potentials more positive than  $V_K$ . Transitions that occur while no current is flowing were investigated indirectly by experiments that instantaneously reveal channel conducting states. The voltage-dependent availability of GIRK1 was examined by measuring  $I_{K,ACh}$  tail current amplitudes after prepulses

that were long enough to achieve steady state activation/deactivation at various membrane potentials.

Fig. 6 shows the relationship between prepulse voltage and normalized tail currents at  $-80$  mV for GIRK1 activated by m2 receptors, by 5-HT<sub>1A</sub> receptors, or directly via G<sub>β1γ2</sub> expression. In each case, the availability of GIRK1 was maximal for prepulses to negative voltages and minimal at voltages near or positive to  $V_K$ . The steady state availability relation was well described by the following Boltzmann function:

$$P_o(V) = I_{\text{tail}}/I_{\text{tail,max}} = 1 - (1 - P_{\text{min}})/[1 + \exp\{z\delta(V_{1/2} - V_m)/kT\}] \quad (2)$$

where  $P_o$  is the relative availability,  $P_{\text{min}}$  is the minimal plateau value owing to incomplete channel deactivation,  $V_{1/2}$  is the potential for half-activation,  $z$  is the valence of the charged gating particle,  $\delta$  is the fractional electrical distance the gating particle moves,  $k$  is Boltzmann's constant, and  $T$  is the absolute temperature. The product of  $z$  and  $\delta$ , the equivalent gating charge, is given in units of electron charge ( $e^-$ ). For m2 receptor activation, 5-HT<sub>1A</sub> receptor activation, and G<sub>β1γ2</sub> expression, values for  $V_{1/2}$  were  $-21 \pm 4$  mV ( $n = 13$ ),  $-20 \pm 4$  mV ( $n = 7$ ), and  $-27 \pm 2$  mV ( $n = 3$ ), respectively. The equivalent gating charge, corresponding to the slope of the relation, was  $1.76 \pm 0.25 e^-$  for m2 receptor activation,  $1.64 \pm 0.18 e^-$  for 5-HT<sub>1A</sub> receptor activation, and  $1.62 \pm 0.13 e^-$  for G<sub>β1γ2</sub> expression. The  $P_{\text{min}}$  values, corresponding to the fractional contribution of  $I_i$ , were  $0.49 \pm 0.05$  for m2 receptor activation,  $0.42 \pm 0.05$  for 5-HT<sub>1A</sub> receptor activation, and  $0.51 \pm 0.03$  for G<sub>β1γ2</sub> expression. The voltage-dependent reduction in  $I_i$  with depolarizing prepulses was accompanied by an increase in both  $I_f$  and  $I_s$  upon reactivation. In all cases,  $I_f$  constituted approximately one third of the deactivated current amplitude and  $I_s$  made up approximately two thirds. In summary, the voltage-dependent activation parameters of GIRK1 were not significantly different among the different methods of G protein activation. This result suggests that the voltage-dependent gating occurs at a point distal to the receptor-G protein activation step.

#### *Voltage-dependent Gating of GIRK1 Is Not Due to Voltage-dependent G Protein Coupling*

The voltage dependence of GIRK1 activation/reactivation does not depend on the method used to activate G proteins. According to present concepts, both m2 receptor activation and 5-HT<sub>1A</sub> receptor activation result in the liberation of endogenous G<sub>βγ</sub> subunits, which activate GIRK1 by a membrane-delimited pathway. Therefore, results thus far indicate only that GIRK1 kinetics do not distinguish between activation by the heterologously expressed G<sub>β1γ2</sub> subunits and endogenous *Xenopus* G<sub>βγ</sub> subunits. We therefore asked whether the voltage-dependent activation could reflect voltage-dependent G protein-channel coupling, as proposed for Ca<sup>2+</sup> channels during G protein-mediated inhibition (see Anwyl, 1991). Currently, there are no direct means to test the voltage dependence of G<sub>βγ</sub>-GIRK1 interaction. Therefore, the most appropriate tactic was to determine the voltage-dependent activation properties of GIRK1 during various levels of receptor activation. If the dissociation constant for G<sub>βγ</sub> coupling to GIRK1 is reduced at positive potentials, which could

account for the reduced GIRK1 availability at positive voltages, the voltage-dependent GIRK1 availability curve would be expected to shift toward more negative membrane potentials at low agonist concentrations ( $<EC_{50}$ ).

Fig. 7 A shows the current trace from a cumulative ACh dose-response experi-

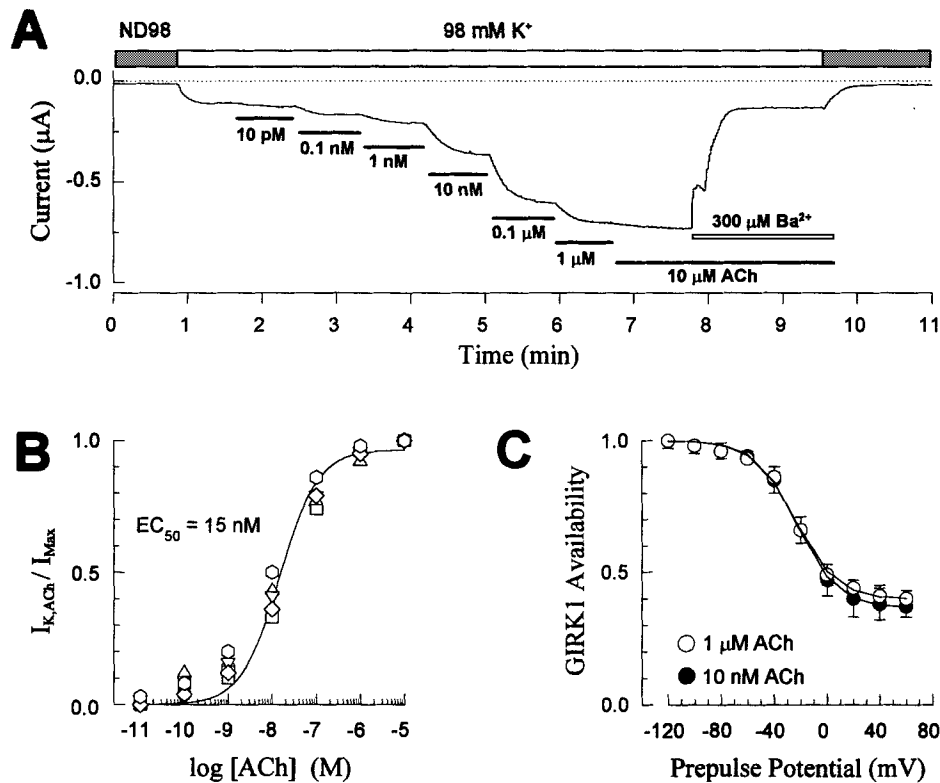


FIGURE 7. Effect of agonist concentration on voltage-dependent  $I_{KACh}$  availability. (A) Cumulative ACh dose-response experiment for an oocyte expressing m2 receptors and GIRK1. Increasing concentrations of ACh (solid bars) were superfused via the U-tube apparatus (see Methods). Subsequent bath perfusion with 300  $\mu$ M Ba<sup>2+</sup> (open bar) completely blocked the ACh-evoked inward current. The small spike during Ba<sup>2+</sup> treatment is a bath perfusion artifact resulting from the transition from U-tube superfusion. (B) Normalized ACh dose-response relations from six separate oocytes. The solid curve is a least-squares fit of the data points according to the Hill equation:  $I_{KACh}/I_{Max} = 1/(1 + ([ACh]/EC_{50})^n)$ , where the  $EC_{50}$  was 15 nM. (C) Voltage-dependent  $I_{KACh}$  availability during GIRK1 activation by 10 nM (filled circles) and 1  $\mu$ M (open circles) ACh. Data points are the mean  $\pm$  SD from four and three oocytes, respectively. (Solid curves) Boltzmann functions fit to the mean data points as described in the text.

ment for GIRK1 activation, and Fig. 7 B shows the normalized dose-response relation. We have fitted the dose-response data to the Hill equation with an  $EC_{50}$  of  $15 \pm 5$  nM ( $n = 6$ ) and a Hill coefficient ( $n_H$ ) of 1.0. The  $EC_{50}$  for ACh activation of  $I_{KACh}$  in atrial cells is  $\sim 24$  times higher than that for the present data on oocyte ex-

pression (Karschin, Ho, Labarca, Elroy-Stein, Moss, Davidson, and Lester, 1991) and may arise from differences at some point in the transduction pathway for oocytes vs myocytes. Progressive  $I_{K_{ACh}}$  desensitization during the cumulative dose-response protocol may also distort the dose-response relation, although we have not systematically studied this question. For this study, the important point is that the steady state voltage-dependent GIRK1 availability parameters during receptor activation by 10 and 100 nM ACh were indistinguishable from those during activation by 1  $\mu$ M ACh (Fig. 7C). In addition, the kinetics of voltage-dependent GIRK1 activation were not altered by the level of receptor activation (data not shown). Thus,  $G_{\beta\gamma}$  coupling to GIRK1 does not appear to be significantly voltage dependent.

The GIRK1 current relaxations are also not due to a voltage-dependent agonist-receptor interaction. After a rapid change in agonist concentration ( $<1$  s), GIRK1 currents developed with a time constant of  $\sim 8$  s (Fig. 8). Therefore, a voltage-dependent agonist-receptor interaction would produce current changes on a time scale of 10–50 s, rather than the 50–500-ms range of the present relaxation experiments.

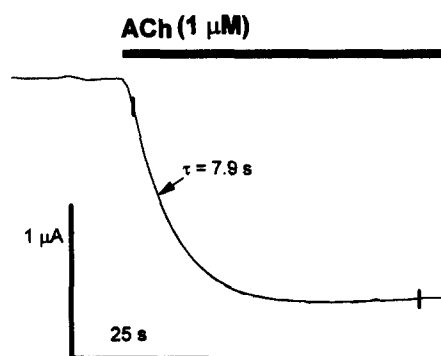


FIGURE 8. Time course for ACh activation of GIRK1. Rapid application of ACh (1  $\mu$ M) to an oocyte coexpressing m2 receptors and GIRK1 and voltage clamped at  $-80$  mV. The time course for complete solution change was  $<1$  s. The region of the waveform between the two vertical lines was fitted to a single exponential (time constant, 7.9 s) plus a linearly sloping baseline.

The experiment of Fig. 8 deserves further comment. In most experiments on  $I_{K_{ACh}}$  in atrial myocytes, concentration jumps at the muscarinic receptor lead to conductance relaxations with time constants of  $\sim 300$  ms (see, for instance, Nargeot, Lester, Birdsall, Stockton, Wassermann, and Erlander, 1982). The experiment of Fig. 8 shows a much slower time constant, although data for ligand-gated channels expressed in oocytes show that our superfusion system has a time constant of  $<1$  s (Cohen et al., 1995). We have found that GIRK1 responses to concentration jumps of ACh do become considerably faster for larger m2 receptor cRNA injections. We have not systematically investigated these effects; but the important point is that, under the present conditions, a voltage-dependent agonist-receptor interaction does not explain the relaxations.

#### *K<sup>+</sup>-dependent Gating of GIRK1*

As for other  $K_{ir}$  channels, the voltage-dependent gating properties of GIRK1 were dependent on the external  $K^+$  concentration ( $[K^+]_o$ ), shifting with respect to  $V_K$ . Fig. 9 shows the effects of reducing  $[K^+]_o$  by fivefold, to 20 mM, on the gating of

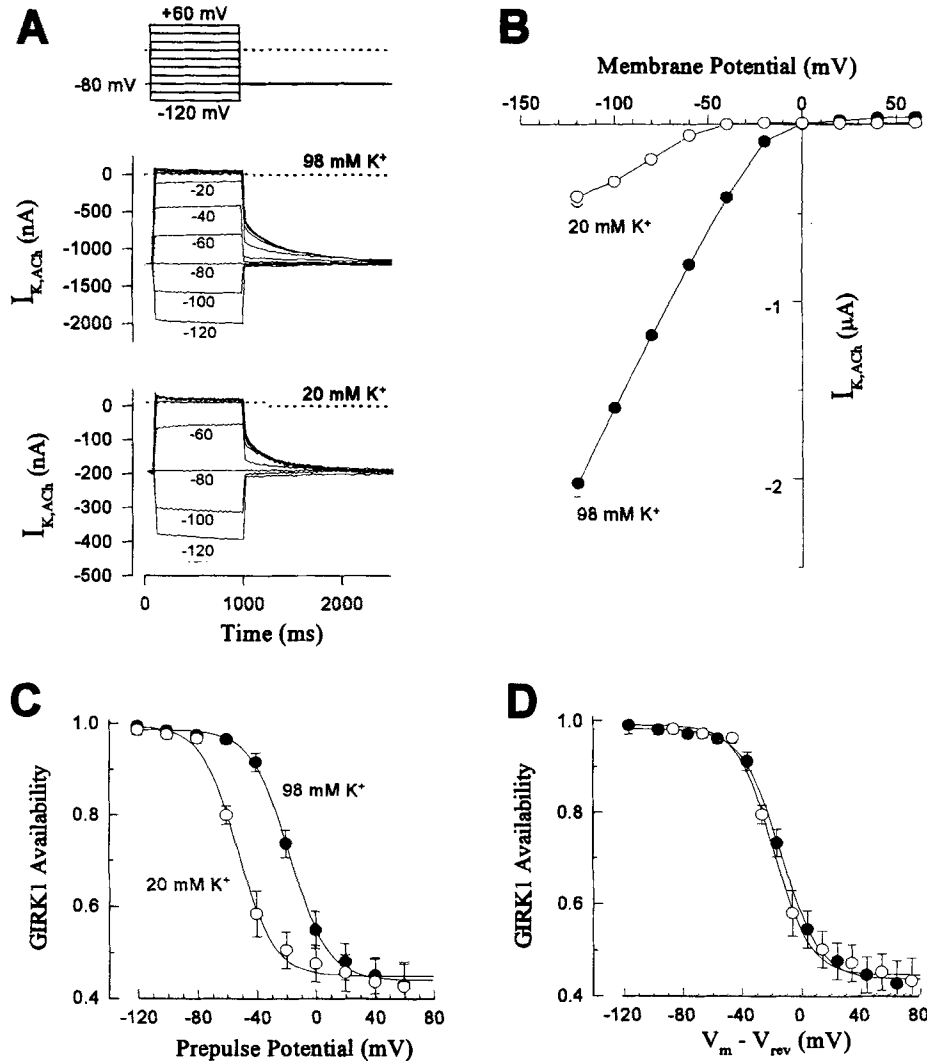


FIGURE 9. External  $K^+$  shifts the voltage dependence of intrinsic GIRK1 gating. (A)  $I_{K_{ACH}}$  during jumps to varying test potentials in 98 mM  $K^+$  (upper traces) and 20 mM  $K^+$  (lower traces). (B) Steady state  $I_{K_{ACH}}$  ( $V$ ) relations in 98 mM  $K^+$  (filled circles) and 20 mM  $K^+$  (open circles).  $V_{rev}$  for  $I_{K_{ACH}}$  was obtained by interpolation between data points and agreed with the predicted  $V_K$  values calculated from the Nernst relation assuming an intracellular  $K^+$  concentration of 90 mM. (C) Steady state voltage-dependent GIRK1 availability in 98 mM  $K^+$  (filled circles) and 20 mM  $K^+$  (open circles) as determined from tail current measurements (see Fig. 6). The solid curves are Boltzmann functions fit to the mean data values; parameters are described in the text. Data are the mean  $\pm$  SD ( $n = 7$ ). (D) Steady state GIRK1 availability curves in C after shifting the voltage axis so that it represents  $V_m - V_{rev}$ .

$I_{K,ACH}$ . Isotonic conditions were maintained with either  $Na^+$  or *N*-methyl-D-glucamine substitution.  $V_{rev}$  for  $I_{K,ACH}$  shifted from  $4 \pm 6$  mV in 98 mM  $[K^+]_o$  to  $-36 \pm 5$  mV in 20 mM  $[K^+]_o$ , which is in excellent agreement with the 40-mV shift expected from a fivefold decrease in  $[K^+]_o$ . Analysis of the voltage-dependent  $I_{K,ACH}$  availability relation in 20 mM  $[K^+]_o$  yielded a  $V_{1/2}$  of  $-55 \pm 3$  mV and an equivalent gating charge of  $1.90 \pm 0.26 e^-$ . Relative to  $V_K$ , the  $V_{1/2}$  value in 20 mM  $[K^+]_o$  ( $V_K - 19$

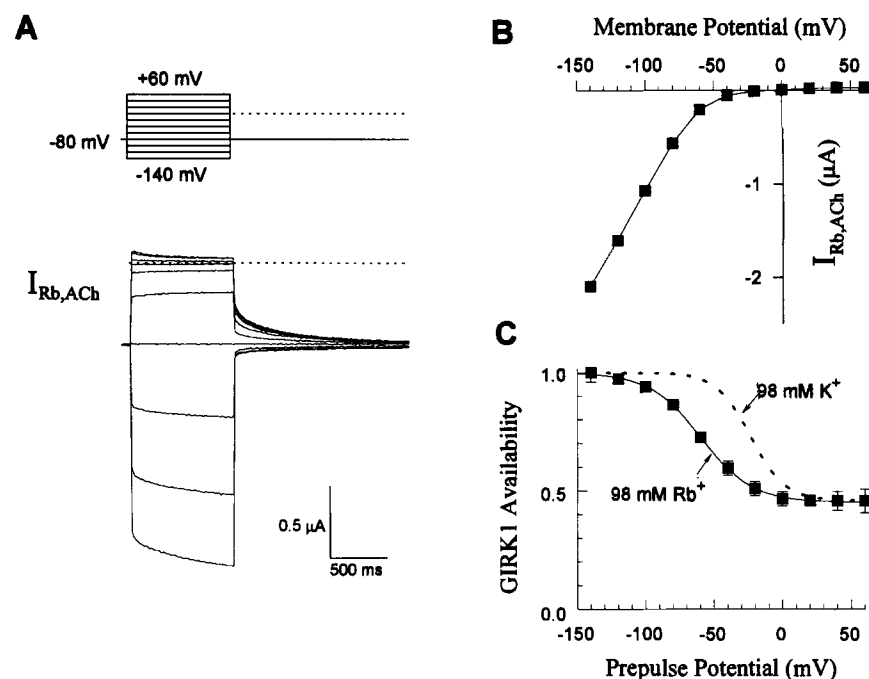


FIGURE 10. Voltage-dependent gating of GIRK1 with  $Rb^+$  as the permeant cation. (A) Steady state ACh-activated  $Rb^+$  currents evoked by voltage steps from a holding potential of  $-80$  mV to various membrane potentials between  $+60$  and  $-120$  mV. The external  $Rb^+$  concentration was 98 mM. (B) Steady state  $I_{Rb,ACH}$  ( $V$ ) relation.  $I_{Rb,ACH}$  amplitudes were measured near the end of each voltage step. (C) Voltage-dependent  $I_{Rb,ACH}$  availability. Normalized  $I_{Rb,ACH}$  tail currents were measured isochronally 12 ms after the voltage was jumped to  $-80$  mV after the 900-ms prepulse steps. Data (filled squares) are the mean  $\pm$  SD from four oocytes. (Solid curve) Boltzmann function fit to the mean values as described in the text. For comparison, the broken curve is GIRK1 availability in 98 mM  $[K^+]_o$  as shown in Fig. 9 D.

mV) was not significantly different from that obtained in 98 mM  $[K^+]_o$  ( $V_{1/2} = V_K - 21$  mV), nor were the  $z\delta$  values (Fig. 9 D). Interestingly, the activation rates for GIRK1 activation were not significantly different in 98, 20, or 10 mM  $[K^+]_o$ , though the weak voltage dependence of  $\tau_s$  appeared to shift with respect to  $V_K$ . These results demonstrate that the voltage-dependent gating of GIRK1 is a function of  $[K^+]_o$ , which is characteristic of other  $K_r$  channels.

To explore the  $K^+$  dependence of gating further, voltage-dependent GIRK1 avail-

ability was examined in the absence of  $[K^+]_o$  using 98 mM external  $Rb^+$  as the permeant cation. From the difference in the  $I_{Rb,ACh}$  and  $I_{K,ACh}$  reversal potentials ( $\Delta V_{rev} = V_{Rb,rev} - V_{K,rev} = -8.5 \pm 1.1$  mV), the GIRK1 permeability ratio of  $Rb^+$  to  $K^+$  ( $P_{Rb}/P_K$ ) was calculated using the following relation from Hille (1992):

$$\Delta V_{rev} = V_{Rb,rev} - V_{K,rev} = (RT/zF) \ln(P_{Rb} [Rb^+]_o / P_K [K^+]_o) \quad (3)$$

where  $P_{Rb}/P_K$  was determined to be  $0.72 \pm 0.03$  ( $n = 4$ ). Fig. 10 shows that in 98 mM  $[Rb^+]_o$ , ACh activated inward  $Rb^+$  currents ( $I_{Rb,ACh}$ ) with characteristic inward rectification and slow activation. Furthermore, the rates of  $I_{Rb,ACh}$  activation ( $\tau_f = 75 \pm 10$  ms,  $\tau_s = 472 \pm 16$  ms) were not significantly different from the rates of  $I_{K,ACh}$  activation ( $\tau_f = 76 \pm 1$  ms,  $\tau_s = 425 \pm 30$  ms) at  $-80$  mV ( $n = 4$ ). The voltage-dependent  $I_{Rb,ACh}$  availability curve, however, was significantly shifted to more negative potentials similar to that seen with low  $[K^+]_o$ ; the  $V_{1/2}$  value was  $-60 \pm 4$  mV. The  $V_{1/2}$  value relative to  $V_{rev}$  was also significantly more negative (so that  $V_{1/2} = V_{rev} - 49$  mV) compared with  $K^+$ -dependent gating ( $V_{1/2} = V_{rev} - 20$  mV). The equivalent gating charge for the  $I_{Rb,ACh}$  availability curve ( $z\delta = 1.3 \pm 0.3 e^-$ ) was also significantly less than that for  $I_{K,ACh}$ . That  $Rb^+$  acts qualitatively like low  $K^+$ , shifting both  $V_{rev}$  and  $V_{1/2}$  to more negative potentials, suggests that external  $K^+$  shifts the voltage dependence of GIRK1 gating positively in a concentration-dependent manner and contributes to or increases the equivalent gating charge of the intrinsic gating mechanism.  $Rb^+$  would substitute only partially for  $K^+$  in these interactions.

## DISCUSSION

### *Slow Activation/Deactivation of GIRK1 Is Analogous to Intrinsic $K_{ir}$ Channel Gating*

The results of our study indicate that the voltage-dependent relaxations of GIRK1 currents result from an intrinsic gating process that takes place entirely at the channel protein, rather than from extrinsic factors such as voltage-dependent G protein-channel coupling or agonist-receptor coupling. Evidence supporting this conclusion is as follows. First, three different methods of G protein activation did not alter GIRK1 relaxation properties. GIRK1 activation via m2 receptors, 5-HT<sub>1A</sub> receptors, and heterologously expressed  $G_{\beta 1-\gamma 2}$  subunits produced GIRK1 currents with equivalent voltage-dependent gating kinetics. Second, the level of G protein activation (as controlled by varying the agonist concentration at the G protein-coupled receptor) did not alter the GIRK1 gating kinetics, as predicted if voltage-dependent G protein-GIRK1 coupling mediated the relaxations. Third, external  $K^+$  shifted voltage-dependent GIRK1 gating in a manner characteristic of intrinsic  $K_{ir}$  channel gating.

We have used the term "intrinsic" operationally, as has been conventional for describing similar phenomena in other  $K_{ir}$  channels. It should be clear, however, that the physical determinants responsible for voltage-dependent GIRK1 gating may indeed be extrinsic to the channel protein itself, in particular  $K^+$  ions (Ciani et al., 1978; Hille and Schwarz, 1978),  $Mg^{2+}$  ions (Matsuda, 1991), and/or intracellular polyamines (Ficker et al., 1994; Lopatin et al., 1994; Fakler et al., 1994) interacting



in a voltage-dependent manner with the channel. Our results further support the recent findings that GIRK1 is gated via  $G_{\beta\gamma}$  dimers and not by  $G_{\alpha}$  subunits (Reuveny, Slesinger, Inglese, Morales, Iniguez-Lluhi, Lefkowitz, Bourne, Jan, and Jan, 1994; Takao, Yoshi, Kanda, Kokubun, and Nukada, 1994; Lim, Dascal, Labarca, Davidson, and Lester, 1995) and therefore support a similar  $G_{\beta\gamma}$  coupling mechanism in atrial myocytes (Logothetis et al., 1987; Ito et al., 1992; Wickman et al., 1994; Yamada et al., 1994) as well as in neuronal cells that express GIRK1 (Kubo et al., 1993; Dascal et al., 1993; Karschin, Schreibleymer, Dascal, Lester, Davidson, and Karschin, 1994). Although our results indicate that the coupling of GIRK1 and  $G_{\beta\gamma}$  dimers is not voltage dependent, they do not exclude the potential influence of bound  $G_{\beta\gamma}$  dimers in the manifestation of slow channel kinetics.

#### *Comparison of GIRK1 Relaxations with Atrial $I_{K_{ACH}}$ Relaxations*

The voltage-dependent relaxations of GIRK1 agree well with the  $I_{K_{ACH}}$  relaxations previously described in acutely isolated frog atrial myocytes (Simmons and Hartzell, 1987). In frog atrial myocytes,  $I_{K_{ACH}}$  relaxations display an instantaneous component followed by a biexponential time-dependent component with time constants of  $\sim 20$  and  $\sim 300$  ms at  $21\text{--}23^{\circ}\text{C}$ . The two time constants in frog atrial cells also depend weakly on voltage and follow a sigmoidal relation. Slow  $I_{K_{ACH}}$  relaxations have also been described in guinea pig atrial myocytes ( $\tau$  range, 50–200 ms at  $35\text{--}37^{\circ}\text{C}$ ) (Iijima et al., 1985) and rabbit sinoatrial node cells ( $\tau$  range, 50–150 ms at  $35\text{--}37^{\circ}\text{C}$ ) (Noma and Trautwein, 1978). Given the high  $Q_{10}$  values ( $>2.5$ ) described for the intrinsic gating of other  $K_{ir}$  currents (Leech and Stanfield, 1981; Ishihara et al., 1989), the fast  $I_{K_{ACH}}$  relaxation component identified in frog atrial myocytes and for GIRK1 may have been too fast to resolve at the higher recording temperatures used in the mammalian studies.

#### *Comparison of Intrinsic GIRK1 Gating with Other $K_{ir}$ Channels*

Intrinsic gating of GIRK1 and its homologues in native tissue differs from that for other  $K_{ir}$  channels in several respects. The first is the presence of three kinetic components in voltage-jump relaxations ( $I_i$ ,  $I_f$ , and  $I_s$ ) vs two for other  $K_{ir}$  channels ( $I_i$  and an  $I_f$  with a  $\tau < 10$  ms; see the following discussion). Our interpretation of the three kinetic components for GIRK1 is the presence of three distinct channel closed or blocked states.

Our experiments provide the most complete kinetic data on the slow activation/deactivation component, which we identify with a long channel closed or blocked time. This component is an unusual property of GIRK1 and its apparent homologues in the atria of other species, as has been described. For constitutively active mammalian  $K_{ir}$  channels, the reported time constants for activation are typically much faster. For the  $K_{ir}$  channel in frog skeletal muscle fibers,  $\tau_{act}$  is  $< 5$  ms at  $13^{\circ}\text{C}$  (Leech and Stanfield, 1981). For the cardiac background  $K_{ir}$  channel ( $i_{K1}$ ),  $\tau_{act}$  is  $< 5$  ms at  $30\text{--}37^{\circ}\text{C}$  (Kurachi, 1985; Tournier, Mitra, Morad, and Rougier, 1987; Harvey and Ten Eick, 1988) and can be slowed down to  $< 10$  ms at  $14\text{--}15^{\circ}\text{C}$  (Saigusa and Matsuda, 1988; Ishihara et al., 1989) and  $< 20$  ms at  $8\text{--}10^{\circ}\text{C}$  (Cohen, DiFrancesco, Mulrine, and Pennefather, 1989). For the  $K_{ir}$  channel current in bovine pulmonary endothelial cells,  $\tau_{act}$  is  $< 5$  ms at  $20\text{--}23^{\circ}\text{C}$  (Silver and DeCoursey, 1990).

Slow rates of activation, however, have been reported for invertebrate  $K_{ir}$  currents in starfish ( $\tau_{act} < 400$  ms at 21–22°C) (Hagiwara, Miyazaki, and Rosenthal, 1976) and *Neanthes* oocytes ( $\tau_{act} < 250$  ms at 22°C) (Gunning, 1983). The GIRK1 component characterized by  $\tau_s$  is also unique among vertebrate  $K_{ir}$  channels in that it is weakly voltage dependent and shows a sigmoidal  $1/\tau_s(V)$  curve (Fig. 4). The only other known  $K_{ir}$  channel current displaying a similar sigmoidal  $\tau_{act}(V)$  relation is the  $K_{ir}$  conductance in oocytes from the marine worm *Neanthes arenaceodentata* (Gunning, 1983).

Similar to other  $K_{ir}$  channels, the voltage-dependent availability of GIRK1 is a function of  $V_K$ . The value for  $V_{1/2}$ , relative to  $V_K$ , therefore constitutes an appropriate parameter for comparisons of gating among  $K_{ir}$  channels. The GIRK1  $V_{1/2} - V_K$  value,  $-20$  mV, is more negative than that for most other  $K_{ir}$  channels. For example, the  $V_{1/2} - V_K$  value for intrinsic gating of the background cardiac  $K_{ir}$  channel is  $-7$  mV (Kurachi, 1985; Saigusa and Matsuda, 1988; Ishihara et al., 1989; Oliva, Cohen, and Pennefather, 1990). For  $K_{ir}$  channels in skeletal muscle fibers, the  $V_{1/2} - V_K$  value is  $-25$  mV in frog dorsal head semitendinosus muscle (Hestrin, 1981) and  $-11$  mV in frog sartorius muscle (Leech and Standen, 1981). For the endothelial cell  $K_{ir}$  channel, the value is  $-8$  mV (Silver and DeCoursey, 1990). In invertebrate cells, the  $V_{1/2} - V_K$  value for the  $K_{ir}$  conductance in starfish eggs is  $-16$  mV (Hagiwara et al., 1976), and it is  $+5$  mV for the  $K_{ir}$  conductance in *Neanthes* oocytes (Gunning, 1983).

For excitable cells, a  $K_{ir}$  conductance having a more negative  $V_{1/2} - V_K$  value would be more readily shut off during membrane depolarization and action potential firing and thereby may better preserve intracellular  $K^+$  levels (Hille, 1992). For  $V_{1/2} - V_K$  values closer to the resting membrane potential, such as the constitutively active  $K_{ir}$  channels, channel activity would be more readily increased during locally elevated  $[K^+]_o$ , causing external  $K^+$  ions to be transported into the cell. This external  $K^+$  "siphoning" or "buffering" role has been proposed for the constitutively active  $K_{ir}$  channels in glia (Barres, Chun, and Corey, 1990) and macrophage (McKinney and Gallin, 1988). Such a maintenance role seems less likely for the highly regulated GIRK1.

The effects of  $Rb^+$  on intrinsic  $K_{ir}$  channel gating have been examined for  $i_{K1}$  in guinea pig ventricular myocytes (Mitra and Morad, 1991) and for the  $K_{ir}$  conductance in bovine pulmonary endothelial cells (Silver, Shapiro, and DeCoursey, 1994). In both cases,  $\tau_{act}$  was increased when  $Rb^+$  was the sole permeant cation versus  $K^+$ , whereas with GIRK1 in the present study, neither  $\tau_f$  nor  $\tau_s$  was significantly different with  $Rb^+$  as the permeant cation compared with  $K^+$ . This difference may be due to the greater voltage dependence of activation exhibited by constitutively active  $K_{ir}$  channels. Interestingly, the relation between availability and voltage, as revealed by GIRK1 tail currents, was significantly more negative for  $I_{Rb,ACH}$  vs  $I_{K,ACH}$ . For the  $K_{ir}$  currents in endothelial cells,  $Rb^+$  similarly dissociates channel gating from the  $V_{1/2} - V_{rev}$  rule; however,  $V_{1/2}$  shifts positive to  $V_{rev}$  ( $V_{1/2} - V_{rev} = +7$  mV, 160 mM  $[Rb^+]_o$ ) compared with the negative displacement in 160 mM  $[K^+]_o$  ( $V_{1/2} - V_{rev} = -7$  mV). In contrast, for GIRK1,  $V_{1/2}$  is shifted further negative from  $V_{rev}$  in high  $Rb^+$  ( $V_{1/2} - V_{rev} = -49$  mV, 98 mM  $[Rb^+]_o$ ) compared with the already negative displacement from  $V_{rev}$  in  $K^+$  ( $V_{1/2} - V_{rev} = -20$  mV, 98 mM  $[K^+]_o$ ). These various

differences in the intrinsic gating properties of GIRK1 and other  $K_{ir}$  channels may reveal basic mechanistic differences among the  $K_{ir}$  channel family.

#### *Implications for Structure-Function Studies*

The functional differences between  $K_{ir}$  channels and outwardly rectifying voltage-gated  $K^+$  channels ( $K_v$  channels) were noted long before knowledge of their different molecular structures. The recent cloning of several  $K_{ir}$  channels (for review see Doupnik, Davidson, and Lester, 1995) indicates little or no sequence homology with  $K_v$  channels with the exception of an  $\sim 18$  amino acid segment termed the pore region that mediates several pore properties in  $K_v$  channels (see Jan and Jan, 1992; Brown, 1993; Pongs, 1993). Members of the  $K_{ir}$  channel gene family possess two putative transmembrane (TM) domains per subunit, in contrast to six for each  $K_v$  channel subunit. The conserved pore region resides between TM1 and TM2 in  $K_{ir}$  channels and between TM5 and TM6 in  $K_v$  channels. Because four  $K_v$  channel subunits are known to coassemble to form a functional channel, the subunit stoichiometry for  $K_{ir}$  channels, although not yet known, is presumed to be four.

Several mechanisms that involve external  $K^+$  binding and internal  $Mg^{2+}$  block have been proposed to explain the intrinsic gating and inward rectifying properties of  $K_{ir}$  channels (Hille and Schwarz, 1978; Ciani et al., 1978; Standen and Stanfield, 1978; Matsuda, 1991; Pennefather, Oliva, and Mulrine, 1992). Now that several cloned  $K_{ir}$  channels are available, structure-function studies are beginning to provide new insights into the underlying molecular determinants of  $K_{ir}$  channel gating (see Doupnik et al., 1995). Recently, the intrinsic gating of cloned constitutively active  $K_{ir}$  channels was found to be controlled by a single residue in TM2 that also affected intracellular block by  $Mg^{2+}$  (Stanfield, Davies, Shelton, Sutcliffe, Khan, Brammer, and Conley, 1994; Lu and MacKinnon, 1994; Wible, Taglialatela, Ficker, and Brown, 1994) and polyamines (Ficker et al., 1994; Lopatin et al., 1994; Fakler et al., 1994). These findings provide strong evidence for extrinsic channel block as the mechanism underlying the intrinsic gating phenomenon for these  $K_{ir}$  channels. The weak voltage dependence of the slow GIRK1 activation/deactivation rates, however, suggests that other processes may be involved. In preliminary studies, we have indeed identified residues in a different region, the putative pore domain, contributing to the slow intrinsic gating of GIRK1 (Doupnik, Kofuji, Davidson, and Lester, 1994b).

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